

CANCER NANOMEDICINE: UTILIZING THE ENHANCED PERMEABILITY AND RETENTION (EPR) EFFECT TO DELIVER HIGH PAYLOADS OF CHEMOTHERAPEUTIC AGENTS DIRECTLY TO TUMOR SITES

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ABSTRACT

The enhanced permeability and retention (EPR) effect serves as the primary scientific basis which supports nanomedicine methods for cancer drug delivery. The EPR effect which Matsumura and Maeda first described in 1986 occurs because solid tumors develop abnormal blood vessels and do not function properly to drain lymphatic fluids. The study investigates how biological mechanisms of EPR effect to control nanoparticle platforms show different clinical application results. The study investigates how passive EPR-based targeting is improved through three methods which include active ligand-mediated targeting and stimuli-responsive release mechanisms and surface engineering techniques that use PEGylating and charge modulation. The analysis shows that EPR heterogeneity between different tumor types and patient groups together with immunological nanoparticle clearance and tumor microenvironment obstacles create a major difference between preclinical research results and actual clinical outcomes. The study evaluates new methods for improving EPR utilization which include vascular normalisation methods and ultrasound-based permeation techniques and artificial intelligence-based formulation design methods. The study ends with a perspective which describes how EPR-based nanomedicine will develop into customized cancer treatment.

Keywords: Cancer Nanomedicine, Epr Effect, Nanoparticle Drug Delivery, Chemotherapy, Tumor Vasculature, Liposomes, Polymer Nanoparticles, Pegylation, Active Targeting, Tumour Microenvironment

INTRODUCTION

The World Health Organization reports that cancer is the second most common cause of death worldwide because it leads to about 10 million fatalities each year. The development of new therapies during the past 50 years has not produced effective treatments because traditional systemic chemotherapy methods still cause severe side effects that result from the way body-wide toxic drugs spread. The small-molecule chemotherapeutic agents doxorubicin and paclitaxel and cisplatin produce genotoxic and cytotoxic effects that damage both cancerous and healthy rapidly dividing cells which leads to blood disorder and nerve damage and kidney damage and heart damage that limits the maximum safe treatment dose used in hospitals.

Nanomedicine uses nanotechnology principles to develop medical treatments which create a new method of drug delivery that enables scientists to solve the drug absorption problems faced by standard chemotherapy treatment. The use of 10-200 nm diameter engineered nanoparticles enables scientists to create a drug delivery method which makes use of the special medical characteristics that exist within tumor tissues to deliver drugs directly to cancerous areas. The EPR effect serves as the main mechanism that allows drugs to build up in specific areas because it explains how large drug carriers exit blood vessels through tumor blood vessel leakage while their escape routes through lymphatic systems remain blocked.

The Enhanced Permeability and Retention effect which Matsumura and Maeda demonstrated through their research on SMANCS macromolecular conjugate, which specifically targets tumor cells, has developed into the main theoretical basis which researchers use to study how nanoparticles deliver drugs. The 1995 approval of Doxil which uses EPR to deliver treatments, established EPR as a method for improving therapeutic outcomes through increased drug delivery to tumors. The study of EPR biology has become an extensive research field which started from EPR biology research in the 1990s, but EPR-targeted nanomedicines have only produced small benefits compared to what preclinical studies expected.

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The review presents current scientific knowledge about EPR effect mechanisms and examines nanoparticle systems that use this effect and assesses clinical data and investigates upcoming developments in EPR enhancement and personalized nanomedicine. The article presents an evidence-based evaluation which shows the field's major achievements and its remaining difficulties.

BIOLOGICAL BASIS OF THE EPR EFFECT

2.1 Tumor Vasculature Aberrations

The EPR effect occurs because solid tumors require abnormal blood vessel growth to support their development. Tumors that reach a size between 1 and 2 millimeters across face oxygen supply limitations which lead to hypoxia-inducible factor-1 α (HIF-1 α) activation and subsequent production of pro-angiogenic substances that include vascular endothelial growth factor (VEGF) and fibroblast growth factor (FGF) and platelet-derived growth factor (PDGF). The newly formed blood vessel network displays both structural and functional irregularities because its pathways create winding routes that develop random connection points which produce endothelium gaps measuring between 100 and 800 nanometers instead of the normal capillary endothelium gap size of 5 to 10 nanometers that results in vascular leakage through fenestrations and vesiculovacuolar organelles.

The permeability properties of EPR emerge from these structural deficiencies because inter-endothelial gaps permit 10 to 200 nanometer nanoparticles to pass through while blocking small molecules. The molecular weight threshold above which macromolecules exhibit EPR-mediated accumulation is approximately 40 kDa, which corresponds to a hydrodynamic diameter of approximately 6–8 nm, which matches the renal filtration cutoff that establishes the minimum effective EPR range.

2.2 Impaired Lymphatic Drainage and Retention

The retention component of EPR arises from the failure of tumor-associated lymphatic networks to adequately clear extravasated macromolecules. The lymphatic system in normal tissue functions continuously to remove interstitial proteins and macromolecules which helps maintain tissue homeostasis. Tumors display functionally disabled intratumoral lymphatic systems because of cancer cell growth which compresses these systems and because of the disorganized structure of their tumor mass. The tumor interstitial space becomes a long-term storage area for nanoparticles after their extravasation because they remain in the body for hours to days instead of being removed through lymphatic drainage which would occur in normal body function.

The combination of enhanced vascular permeability and impaired lymphatic clearance produces a passive concentration gradient which results in increased nanoparticle accumulation within tumor tissue. The study used radiolabelled nanoparticles to show that murine tumor models demonstrated tumor-to-muscle accumulation ratios between 5:1 and 50:1 for optimally designed nanoparticles while EPR-targeted delivery produced intratumoral drug concentrations that achieved 10-100 times the levels of free drug at equivalent doses.

2.3 EPR Heterogeneity and Clinical Limitations

The substantial variation of EPR magnitude among different tumor types and individual patients and various tumor parts within a single tumor represents a major challenge that now medical researchers recognize as a crucial drawback of EPR-based methods for drug delivery. The EPR effect shows its strongest expression in tumors that grow rapidly and possess extensive blood vessel networks which include Kaposi's sarcoma and particular forms of breast and ovarian cancer. The effect shows significant reduction because pancreatic ductal adenocarcinoma desmoplastic tumors develop a dense stromal structure that increases interstitial fluid pressure and forces tumor blood vessels to narrow, which results in total hindrance of nanoparticle movement through the tumor. Clinical imaging studies using Evans blue or gadolinium-labelled nanoparticles as EPR surrogates have demonstrated that EPR-mediated tumour accumulation is highly variable across patient cohorts, with a subset of patients showing minimal EPR activity that may explain non-response to nanomedicine-based regimens.

NANOPARTICLE PLATFORMS FOR EPR-MEDIATED DELIVERY

3.1 Liposomes

Liposomes serve as the most advanced drug-delivery particle system in medical use because they have been the main method through which EPR-based chemotherapy delivery systems reached medical application. Liposomes consist of spherical vesicles that have a lipid bilayer structure and measure between 50 and 200 nanometers in diameter, which enables them to store hydrophilic drugs within their water-based center and hydrophobic drugs inside their lipid

bilayer structure. The prototype nanomedicine platform emerged from their biocompatibility and biodegradable properties combined with their multiple surface engineering capabilities.

Doxil which uses PEGylated liposomal doxorubicin delivery system became the first US Food and Drug Administration approved nanomedicine and now serves as the standard for EPR-based drug delivery systems. The pharmacokinetic research showed that PEGylation of doxorubicin extended its plasma half-life from 5 hours to more than 55 hours, which created an extended period for EPR-based tumor accumulation to occur. Doxil delivered a 4 times greater drug concentration to tumors while decreasing the risk of cardiotoxicity by 66 percent when compared to free doxorubicin during important clinical studies for Kaposi's sarcoma and ovarian cancer treatment.

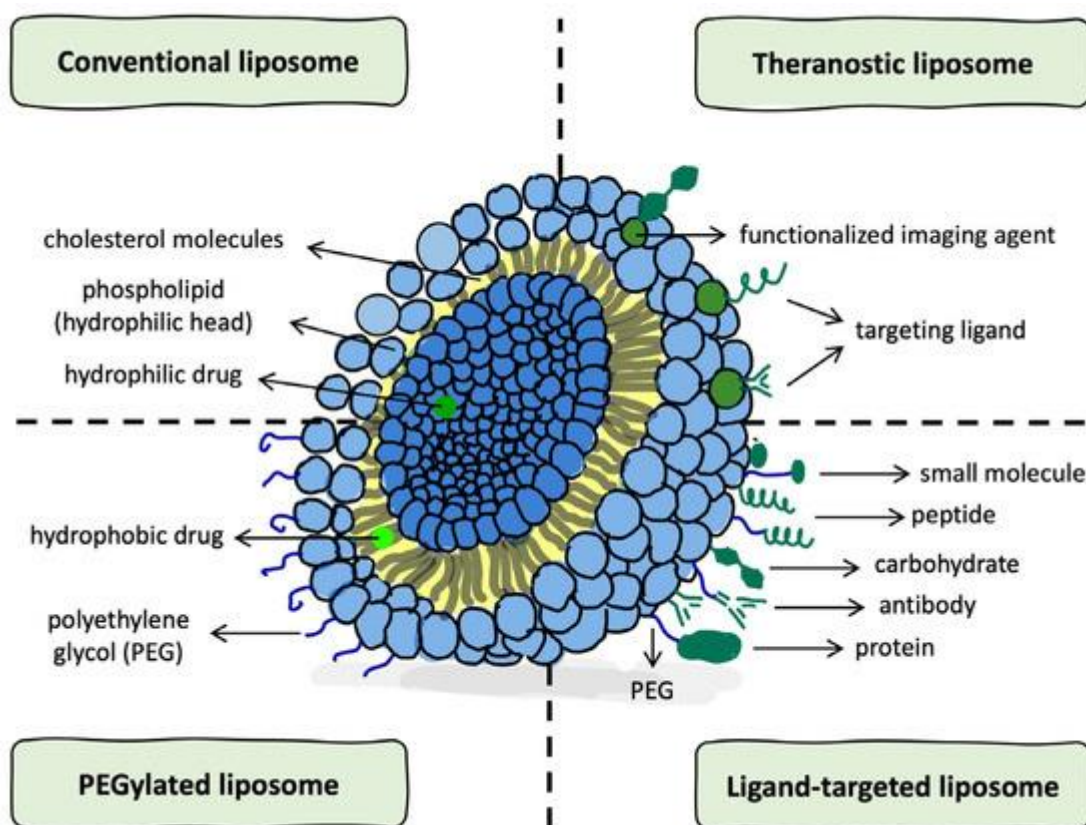


Fig 1-The different liposome-based drug delivery systems: conventional liposome, PEGylated liposome, ligand-targeted liposome, and theranostic liposome.

The multiple liposomal drug formulations that followed Myocet and DaunoXome and Marqibo and Onivyde have been approved for use in different types of cancer treatment which proves the effectiveness of liposomal EPR-based delivery systems. The research currently underway develops thermosensitive liposomes which release their therapeutic contents when exposed to mild local hyperthermia that ranges between 39–42°C. The system enables controlled spatial drug release throughout the entire tumour volume by using combined localized heating methods.

3.2 Polymeric Nanoparticles

Biodegradable polymeric nanoparticles fabricated from materials such as poly(lactic-co-glycolic acid) (PLGA), poly(lactic acid) (PLA), and poly(caprolactone) (PCL) provide adjustable drug release rates through changes in their polymer molecular weight and copolymer composition and nanoparticle design. The characterization of PLGA nanoparticles has reached a high level because the polymer matrix hydrolyzes its ester bonds which release drugs at constant rates for multiple days until three weeks while keeping drug levels above therapeutic limits in tumors for extended times after one dose. Abraxane (nab-paclitaxel) contains a 130 nm albumin-bound paclitaxel nanoparticle which serves as a major clinical demonstration for EPR delivery through polymeric nanoparticles. Abraxane achieved better clinical results than Cremophor EL-solubilised paclitaxel in metastatic breast cancer because it combined albumin receptor-mediated transcytosis with gp60 and SPARC-mediated tumor accumulation and EPR-based drug

delivery, which resulted in a 33% higher objective response rate and lower rates of hypersensitivity reactions. Abraxane obtained authorization for treatment of both non-small cell lung cancer and pancreatic cancer.

3.3 Dendrimers, Inorganic Nanoparticles, and Emerging Platforms

Dendrimers function as macromolecular structures which possess specific branch points and defined chemical properties to create controlled binding sites for drug molecules and targeting ligands and imaging agents. The research studied Polyamidoamine (PAMAM) dendrimers which belong to generation 4 and 5 because they function as drug delivery systems for cisplatin and methotrexate through their PEGylated surface which increases their plasma circulation time and supports EPR-based tumor targeting. The physical characteristics of inorganic nanoparticles which include gold nanoparticles (AuNPs) and iron oxide nanoparticles (IONPs) and mesoporous silica nanoparticles (MSNs) create advantages for their use in drug delivery systems. AuNPs act as both therapeutic agents and diagnostic tools because their near-infrared plasmon resonance absorption facilitates photothermal tumor destruction while delivering doxorubicin after EPR-based tumor accumulation. IONPs function as MRI-visible agents which enable healthcare professionals to use EPR-based tumor confirmation before starting treatment.

SURFACE ENGINEERING STRATEGIES TO AUGMENT EPR EXPLOITATION

4.1 PEGylation and Stealth Properties

The mononuclear phagocyte system (MPS) which consists of liver macrophages (Kupffer cells) and spleen and bone marrow macrophages functions as the main immune defense system which protects against EPR-based nanoparticle delivery methods. Uncoated nanoparticles undergo immediate opsonisation through serum protein binding which includes complement components and immunoglobulins and fibronectin leading to their elimination from the bloodstream within minutes to hours. The PEGylation process involves creating a hydrophilic brush layer through polyethylene glycol chain bonding to the nanoparticle surface which prevents protein adsorption resulting in 10 to 100 times longer plasma half-life through reduced MPS identification. The optimal PEG architecture for stealth effect involves chains of molecular weight 2,000–5,000 Da at surface densities of 0.5–1.0 chains/nm², creating a mushroom-to-brush transition that maximises steric repulsion of opsonins. The 'PEG dilemma' describes how PEG chains help with systemic circulation and EPR-based drug delivery but they obstruct endosomal escape and drug release from nanoparticles in cancer cells. Research currently focuses on zwitterionic surface coatings and polysarcosine materials as alternatives to PEG which can eliminate the existing trade-off.

4.2 Active Targeting with Ligand Conjugation

Active targeting strategies which use receptor-mediated specificity together with the EPR-based accumulation of nanoparticles aim to achieve better tumour cell drug uptake after EPR-mediated extravasation. The targeting ligands which include monoclonal antibodies (immunoliposomes) and antibody fragments (Fab and scFv) and aptamers and peptides (RGD and iRGD) and small molecules (folate and transferrin) bind to nanoparticle surfaces through polyethylene glycol spacers in order to target receptors that tumour cells overexpress on their membranes.

The folate receptor exists in over 90% of ovarian cancers and 50 to 80% of breast cancers and multiple other types of cancer which makes it a valuable target for folate-conjugated nanoparticles. Clinical evaluation of EC145 (vintafolide, a folate-targeted vinca alkaloid conjugate) demonstrated that folate-receptor-positive ovarian cancer patients showed better response rates than their receptor-negative tumour counterparts which established clinical proof for receptor-targeted EPR enhancement. The tumour-penetrating peptide iRGD has gained popularity because it activates transcytosis pathways that enable nanoparticles to move more freely into tumour tissue through blood vessel EPR distribution.

4.3 Stimuli-Responsive Release Systems

The therapeutic efficacy of EPR-accumulated nanoparticles depends on two factors which are their capacity to accumulate in tumors and their ability to release drugs at the tumor location. The development of stimuli-responsive nano formulations enables researchers to use the unique physicochemical properties of solid tumors which include acidic pH levels between 6.0 and 6.8 and elevated glutathione levels between 2 and 10 mM and his bodily matrix metalloproteinase MMP enzymes and tumor air deficiency conditions to release their drugs exclusively inside cancerous tissue. The pH-sensitive liposomes which contain DPSE-PEG2000-succinyl-DOPE formulations release their drugs through membrane destabilisation at tumor extracellular pH values. The disulfide-bridged polymer nanoparticles release their payload when they enter intracellular conditions which contain reductive elements.

CLINICAL TRANSLATION: ACHIEVEMENTS AND CHALLENGES

5.1 Approved Nanomedicines and Clinical Outcomes

The clinical pipeline of EPR-exploiting nanomedicines includes two approved products Doxil and Abraxane and three additional products Genexol-PM which uses polymeric micellar paclitaxel and Nanoxel-M which uses polymer-micellar docetaxel and ThermoDox which uses thermosensitive liposomal doxorubicin which is undergoing multiple regulatory assessments. The results of meta-analyses which tested clinical trials of nanomedicine formulations against their free drug counterparts showed consistent safety profile enhancements which included decreased acute hypersensitivity reactions and decreased cardiotoxicity for anthracycline formulations but showed only slight and inconsistent improvements in efficacy measurement results.

The meta-analysis which Petersen and his team conducted in 2016 identified linkages between 14 randomized controlled trials of liposomal doxorubicin formulations which showed that these treatments reduced the odds of developing cardiotoxicity by 81 percent while showing no impact on progression-free or overall survival across most medical conditions. The study demonstrates the fundamental problem which exists in EPR-based nanomedicine because EPR-based drug delivery methods decrease systemic toxicity through better pharmacokinetics and biodistribution but EPR-based tumor targeting methods do not deliver enough therapeutic benefits to increase survival rates in most tumor types.

5.2 Strategies to Enhance EPR Magnitude

The research on EPR heterogeneity which obstructs nanomedicine success has led scientists to test both drug-based and physical methods which increase EPR levels before or during their nanoparticle treatment. Antiangiogenic treatment with low-dose agents such as bevacizumab and sunitinib seeks to restore abnormal tumour blood vessel structures into typical blood vessel structures which leads to better blood flow and particle distribution even though total blood vessel count decreases. The researchers found that after antiangiogenic treatment the body maintains a 1 to 7 day interval during which blood vessel restoration occurs which results in optimal nanoparticle distribution. The study showed that focused ultrasound and photoacoustic stimulation could temporarily boost tumor blood vessel permeability through microbubble-driven sonoporation which produced an acoustic EPR effect that increased nanoparticle uptake by 3 to 5 times in preclinical studies. The study investigates focused ultrasound combined with thermosensitive liposomes as a treatment for hepatocellular carcinoma which has progressed to Phase II clinical testing.

FUTURE DIRECTIONS IN EPR-TARGETED NANOMEDICINE

6.1 EPR Prediction Biomarkers and Patient Stratification

The clinical testing of EPR-predictive biomarkers for patient classification shows the highest potential impact on upcoming developments within this research area. The proposed EPR magnitude surrogates include three measurements which track plasma VEGF levels and dynamic contrast-enhanced MRI (DCE-MRI) assessments of tumour vascular permeability and positron emission tomography (PET) imaging with radiolabelled folate to measure tumour macrophage density. The upcoming clinical studies need to use EPR biomarker-based patient classification systems to verify whether EPR-high patient subgroups experience significant treatment advantages from nanomedicine compared to standard chemotherapy methods.

6.2 AI-Guided Nanoparticle Design

Machine learning techniques enable scientists to use their existing vast collection of nanoparticle physical and chemical properties data which links to in vivo drug distribution studies as a method for speeding up their work to develop better nanoparticle designs. Deep learning models show their ability to forecast optimal nanoparticle design parameters through their training on datasets which include size zeta potential surface coating density and polymer composition and drug encapsulation efficiency information as it relates to tumour accumulation indices. The AI-powered design system will decrease the experimental process which scientists have used to develop nanoparticle formulations throughout history.

6.3 Bioinspired and Cell-Membrane Coated Nanoparticles

Bioinspired nanoparticles that scientists developed use natural cell membranes from red blood cells and platelets and cancer cells and immune cells to create new methods for extending their active time in the bloodstream while improving their ability to target tumors through their natural biological properties which surpass the effectiveness of synthetic surface coatings. The platelet membrane-coated nanoparticles use their ability to attract platelets to sites of

vascular damage which display collagen-exposed subendothelial matrix, a characteristic that occurs in many tumor blood vessels, to enable their targeted delivery. The cancer cell membrane-coated nanoparticles use self-recognition mechanisms based on homotypic adhesion between similar cancer cell membranes to enable targeted delivery to tumors. The early preclinical data from these platforms show great potential. The translation process needs to solve two challenges, which include scaling manufacturing processes and evaluating immunogenicity.

CONCLUSION

The EPR effect has established a new scientific framework which has enabled cancer nanomedicine research to progress through four decades of development into nanoparticle drug delivery systems which received clinical approval and bettered the therapeutic index for multiple major chemotherapeutic drugs. The EPR-exploiting nanomedicines which reduce toxicity see their benefits reach cancer patients with ovarian cancer and Kaposi's sarcoma and metastatic breast cancer through their ability to demonstrate improved clinical results.

The field needs to conduct an honest assessment of its current situation because researchers have found that passive EPR exploitation functions as an ineffective method for achieving targeted treatment results. The ability of different tumor types and individual patients and their intratumoral regions to develop EPR shows a relationship with tumor microenvironment factors which include high interstitial pressure and dense stroma and immune system mechanisms that track down and destroy foreign bodies.

The path forward requires the combination of multiple approaches which work together with EPR-based patient classification through biomarker predictions and enhanced EPR performance through medical treatments and physical methods and targeted drug delivery which improves tumor cell uptake and drug release through stimuli-responsive systems and artificial intelligence-powered nanoparticle creation. The integration of these methods into personalized nanomedicine will create the most effective solution which matches specific nanoparticle systems and targeting methods and drug release patterns to the unique tumor characteristics of each patient.

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